THE INFLUENCE OF SLOW RECOVERY INSOLE ON PLANTAR PRESSURE AND CONTACT AREA DURING WALKING

ROOZBEH NAEMI*, KIMBERLEY LINYARD-TOUGH, AOIFE HEALY and NACHIAPPAN CHOCKALINGAM

Center for Sport, Health and Exercise Research
Faculty of Health Science, Staffordshire University
Science Center, Leek Road, Stoke-on-Trent ST4 2DE, UK
* r.naemi@staffs.ac.uk

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Plantar pressure assessment is commonly used as a tool to assess the efficacy of insoles in reducing the risk factors associated with soft tissue mechanical trauma during weight bearing activities of daily living. Conformity results in an increase in the contact area between the insole and the foot. Therefore, this is believed to result in a reduction of plantar pressure by distributing the force over a larger area. While high plantar pressure can be relieved by customized insoles that closely fit to the shape of the foot, it has also been shown that the plantar pressure parameters can

1. Introduction

Plantar pressure assessment has been frequently used to assess the insole’s effectiveness in reducing the risk factors associated with soft tissue mechanical trauma during weight bearing activities of daily living. Conformity results in an increase in the contact area between the insole and the foot. Therefore, this is believed to result in a reduction of plantar pressure by distributing the force over a larger area. While high plantar pressure can be relieved by customized insoles that closely fit to the shape of the foot, it has also been shown that the plantar pressure parameters can
also be altered using a flat insole or a footbed that can conform to match the shape or the profile of the plantar surface of the foot.\textsuperscript{2,3} A material known as Poron\textsuperscript{R} (Rogers Corporation) is recognized as being effective in reducing plantar pressure in diabetic neuropathic patients.\textsuperscript{4,5} A variety of Poron materials including a normal (Poron 4708), and a slow rebound variation (Poron 96) are commonly used in clinical practice. Compared to a normal Poron (NP), the slow rebound (SR) Poron is claimed to result in a custom fit during usage and is considered to be more effective in increasing the contact area and in reducing the interface pressure during usage.

In a previous study\textsuperscript{6} a significant difference was reported when the forefoot peak plantar pressure was compared for a SR Poron against a NP insole during walking. However, there is a paucity of studies which consider the effect of the two variations of Poron insole on contact area (CA) and contact pressure (CP) across different regions of the foot.

Furthermore, despite the fact that an increase in CA is believed to reduce the CP, such a relationship has not been previously investigated across different regions of the foot. Such investigation could shed more light on the efficacy of SR Poron compared to a NP and in understanding the mechanism by which the plantar pressure parameters are affected during walking.

2. Aim

This study is aimed at investigating the effectiveness of NP and SR Poron insoles on the CA, and CP at different regions of the foot during walking, and to assess whether the increase in the CA results in a decrease in CP in any of the tested insoles.

3. Method

Nine healthy individuals (five females and four males) with body mass (76.8 ± 24.4kg) and shoe UK size (8 ± 1) participated in this study. Appropriate ethical approval was granted from the Faculty’s Ethics Committee.

The SR and NP flat insoles had 6.35 mm thickness with a Shore O hardness of 18 (Fig. 1). The 6 mm low density ethylene vinyl acetate (EVA) flat insole had Shore A hardness of 25/shore O hardness = 35 and was used as the control (Fig. 1). All insoles were tested in a Plimsoll (Fig. 1).

A commercially available in-shoe pressure measurement system (F-scan, Tekscan Inc., USA) was used to measure the interface pressure between the insole and the plantar surface of the foot, while the participant walked across the lab over a 10 m walkway at their preferred speed (1.3 ± 0.2 m/s). Plantar pressure data was recorded from each foot over five consecutive stance phases during each trial. The data was collected over five trials in each insole condition: The EV (control), SR Poron and the NP. A template was designed to divide the foot into 10 different
regions, including underneath the arch (ARC), center of the midfoot (CMF), center of heel (CHE), Hallux (HAL), heel (HEE), first Metatarsophalangeal joint (FRM), central Metatarsophalangeal joints (CEM), fifth Metatarsophalangeal joint (FIM), and lateral midfoot (LMF) and toes (TOS) (Fig. 1). For each participant the CA and CP were averaged across 25 stance phases for the left and right foot separately. To identify if a significant difference in CA and CP between the three different insole conditions (SR), (NP) and (EV) across the entire foot or the 10 foot regions existed, a repeated measures ANOVA was performed. Furthermore, Pearson product-moment correlation was conducted to determine the relationship between the CA and CP at different regions of the foot when different types of insoles were used. All statistical tests were performed using SPSS (IBM Corp. Released 2013. IBM SPSS Statistics for Windows, Version 22.0. Armonk, NY: IBM Corp) software.

4. Results

4.1. Significant differences ($p < 0.05$)

CA ($SR$ versus $NP$): The CA at the ARC ($\eta^2 = 0.409$, $p = 0.020$) and CMF ($\eta^2 = 0.719$, $p = 0.021$) in SR were significantly higher compared to NP condition (Fig. 2).

CA ($SR$ versus $EV$): The CA at the ARC ($\eta^2 = 0.409$, $p = 0.010$), CMF ($\eta^2 = 0.719$, $p = 0.000$) and LMF ($\eta^2 = 0.592$, $p = 0.000$) in SR were significantly higher compared to EV (Fig. 2).
CA (NP versus EV): There was a significant increase ($\eta^2 = 0.557, p = 0.001$) in the CA for the entire foot in NP ($77.10 \pm 12.98 \text{cm}^2$) compared to EV ($70.19 \pm 11.97 \text{cm}^2$), while CMF ($\eta^2 = 0.719, p = 0.000$) and LMF ($\eta^2 = 0.592, p = 0.012$) had significantly higher CA in the NP compared to EV condition (Fig. 2).

CP (SR versus NP): The CP at ARC region was significantly ($\eta^2 = 0.494, p = 0.010$) higher in SR compared to the NP condition (Fig. 3).

CP (SR versus EV): There was a significant increase in the CP in the ARC ($\eta^2 = 0.494, p = 0.004$), CMF ($\eta^2 = 0.318, p = 0.042$) and LMF ($\eta^2 = 0.296, p = 0.049$) regions in SR as compared to EV condition (Fig. 3).

CP (NP versus EV): For the entire foot, there was a significant decrease ($\eta^2 = 0.386, p = 0.015$) in CP in NP ($65.01 \pm 27.16 \text{kPa}$) compared to EV ($101.16 \pm 28.35 \text{kPa}$) condition (Fig. 3).

4.2. Significant relationships ($p < 0.05$)

NP: There was a significant correlation between CA and CP in NP condition at CHE ($r = 0.701, p = 0.001$), HAL ($r = 0.597, p = 0.009$), HEE ($r = 0.477, p = 0.045$), and FRM ($r = 0.544, p = 0.020$) regions.

SR: Significant correlations were found between CA and CP in SR condition at CHE ($r = 0.734, p = 0.001$), HAL ($r = 0.623, p = 0.006$), HEE ($r = 0.500, p = 0.035$), and FIM ($r = 0.652, p = 0.003$) regions.

EV: It was found that CA and CP were significantly correlated in EV condition at CHE ($r = 0.734, p = 0.001$), HAL ($r = 0.663, p = 0.006$), HEE ($r = 0.592, p = 0.001$), and FRM ($r = 0.544, p = 0.020$) regions.

Fig. 2. (Color online) CA across different regions of the foot for SR, NP, and EV. Significant differences are shown with a bracket.
Both SR and NP, compared to EV, tend to significantly increase CA at CMF and LMF regions. While SR showed to have an increased CA at CMF compared to NP and significantly higher CA at ARC compared to both NP and EV, NP showed a significantly higher CA over the entire foot compared to the EV insole condition.

SR showed a significant increase in the CP at ARC area compared to both EV and NP conditions. Also the SR compared to EV condition seem to cause significantly higher pressure at CMF and LMF. This may have practical implications where increasing pressure at certain regions of the foot is not desirable.

When considering the entire foot, only NP insole significantly increased the CA and decreased the CP compared to EV insole. Tests of relationship showed significant and positive correlations between CA and CP in the HEE, HAL and CHE regions in all tested insoles. For other regions there was no consistent correlations between CA and CP that was valid across all three insole conditions. For example, in NP condition there was a significant positive correlation between CP and CA at FRM, and at FIM in SR condition. Also, positive significant correlations were observed at FRM, FIM, and CEM in EV condition. The fact that no negative correlation was observed between the CA and CP at any plantar region of the foot
for any of the tested insoles, contradicted the expected decrease in CP as a result of the increase in CA. This can be attributed to the thickness of the insoles that were tested in this study and the possibility of these to have bottomed out during the stance phase of walking. This could have resulted in simultaneous increase in the pressure and contact area. More studies are needed in future to investigate the effect of insole thickness on the reported parameters in this study.

6. Conclusion

The results of this study indicated that only NP insole, when compared to the EV insole, increased the CA and decreased the CP on the entire plantar surface of the foot. SR showed to significantly increase CA at ARC and CMF regions compared to NP. The unexpected positive significant correlation between CA and CP were observed at the HEE, HAL and CHE regions for all tested insoles.

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